

# Effect of ultrasound on the setting characteristics of glass ionomer cements studied by Fourier Transform Infrared Spectroscopy

A. Talal · K. E. Tanner · R. Billington ·  
G. J. Pearson

Received: 19 July 2008 / Accepted: 29 August 2008 / Published online: 25 September 2008  
© Springer Science+Business Media, LLC 2008

**Abstract** *Objective* To investigate the effect of ultrasound (US) application, US starting time and US duration on the setting of glass ionomer cement (GIC) by using Attenuated Total Reflectance Fourier Transform Infrared (ATR/FTIR) spectrometer. *Methods* Two conventional GICs, Fuji IX Fast and Ketac Molar were studied. US application was started at 30 s or 40 s after mixing and was applied for times between 15 and 55 s on samples of two different thicknesses. The samples were analysed using ATR/FTIR. *Results* US accelerated the curing process in both cements, US needed to be applied for more than 15 s. Both Fuji IX and Ketac Molar showed increased setting on increasing the US application duration from 15 s to 55 s. Increased setting of the GICs was produced when US application started 40 s after mixing rather than 30 s after mixing. *Conclusions* The significant findings of the study include that US application accelerated the setting processes, by accelerating the formation of the acid salts. The salt formation increased with increase time of US application. The effect of application of US to setting GICs is influenced by time of the start of application of the US. The

effects appear to material specific, with Ketac Molar showing a greater effect than Fuji IX.

## 1 Introduction

Glass ionomer cement (GIC) is widely used as restorative materials in dentistry. They have also been used as bone cements in orthopaedic and ENT surgery because they are bioactive and promote bone growth [1, 2]. In dental applications the important properties are fluoride release, adhesion to tooth structure and negligible volume change during setting. These properties prevent bacterial micro-leakage and subsequent caries progression [3].

However, despite these advantages there are some disadvantages associated with GIC. They are moisture sensitive and have slow maturing processes so there are delays in the development of their final strength. GIC is also susceptible to fracture and has low wear resistance until fully matured [4, 5, 6]. Damage to the cement prior to complete setting leads to long term reduction in the strength of the GIC, thus accelerating the setting of GIC will overcome some of the disadvantages associated with slow setting. Currently GICs have generally been limited in use to the areas of low masticatory forces such as Class III and V restorations [7].

Some improvements have been made in their composition to overcome these problems and to gain a command set. These have included changes in the particle size of the glass phase, the molecular weight of polymer and the development of resin modified glass ionomer cements and cermets. These resin based modified materials have some of the benefits of conventional glass ionomer cements, such as good adhesion to tooth and fluoride release. However

---

A. Talal · K. E. Tanner  
Department of Materials, Queen Mary University of London,  
Mile End Road, London E1 4NS, UK

*Present Address:*

A. Talal (✉) · K. E. Tanner  
Departments of Mechanical and Civil Engineering, University of  
Glasgow, James Watt South Building, Glasgow G12 8QQ, UK  
e-mail: atalal@eng.gla.ac.uk

R. Billington · G. J. Pearson  
Department of Biomaterials in Relation to Dentistry,  
Queen Mary University of London, Mile End Road,  
London E1 4NS, UK

due to the presence of resin these systems also have disadvantages. The resin systems show polymerization shrinkage, monomer toxicity and poor long term mechanical properties particularly abrasion resistance as compared to conventional glass ionomer cements [7, 8].

It has been proposed that by applying US, the setting reaction of glass ionomer cements could be significantly accelerated and the early properties can be substantially increased compared to traditional glass ionomer cements. By accelerating the maturation process, properties such as strength and resistance to water degradation immediately after placement of the filling will be improved. There are potential additional advantages in the use of US such as void reduction and better flow and adaptation of the cement to the cavity. Rapid setting allows a decrease in chair time, making restorations more convenient for both the patient and clinician, while also ensure that the patient can load the restoration sooner without risk of damage [8, 9].

The aim of the work reported here was to follow the setting of GIC when accelerated by the application of ultrasonic excitation and with special emphasis on analyzing the effect of ultrasound starting time and duration of US application after mixing on the setting of GIC.

## 2 Materials and methods

Two conventional chemically cured capsulated GICs, Fuji IX (GC Corporation, Tokyo, Japan, lot number 0503081) and Ketac Molar (3-M ESPE, Seefeld, Germany, lot number 159219) were used. Both the cements consisted of an acid soluble calcium fluoroaluminosilicate glass powder and an acid liquid which is copolymer of itaconic and maleic acid. The powder and liquid are held in separate chambers in precise ratios in a capsule. The capsule is activated and mixed in a triturator. The equipment used for ultrasonically curing GIC was an EMS Piezon Master 400 dental scalar. The tip used for applying ultrasound is shown in Fig. 1 and has a nominal tip diameter of 2 mm. This ultrasonic equipment is routinely used by dentists for de-scaling purposes and it has a frequency between 25 and 30 kHz.

Samples were prepared according to the manufacturer's specifications in a roto mixer (ESPE D-82229, Seefeld, Germany) and were injected in 3 mm and 4 mm deep cavities 3 mm in diameter produced moulds manufactured from polyvinylsiloxane impression material. US was applied 30 or 40 s after mixing by placing the scaler tip on the top of the cement and applying light hand pressure to ensure the tip remained in contact with cement without causing any deformation. Five different durations 15, 25, 35, 45 and 55 s of US were applied. For each of variable,



**Fig. 1** Tip used for ultrasound application

start time, duration and cement type, 3 repeat samples were prepared and analysed.

Samples were examined using a FTIR machine (Perkin-Elmer) in reflectance mode (Golden Gate) using Perkin-Elmer IR spectroscopy software. Immediately after cessation of the US application the moulds were placed on the FTIR machine with the side opposite to that where the US was applied facing the diamond window. The FTIR wavelength range was set between  $1,800\text{ cm}^{-1}$  and  $700\text{ cm}^{-1}$ . To minimize the error 4 scan cycles were used for each reading. Before taking the sample readings, a background spectrum was obtained. This spectrum is a single-beam spectrum recorded without a sample on the machine, and used in ratio calculations for sample readings.

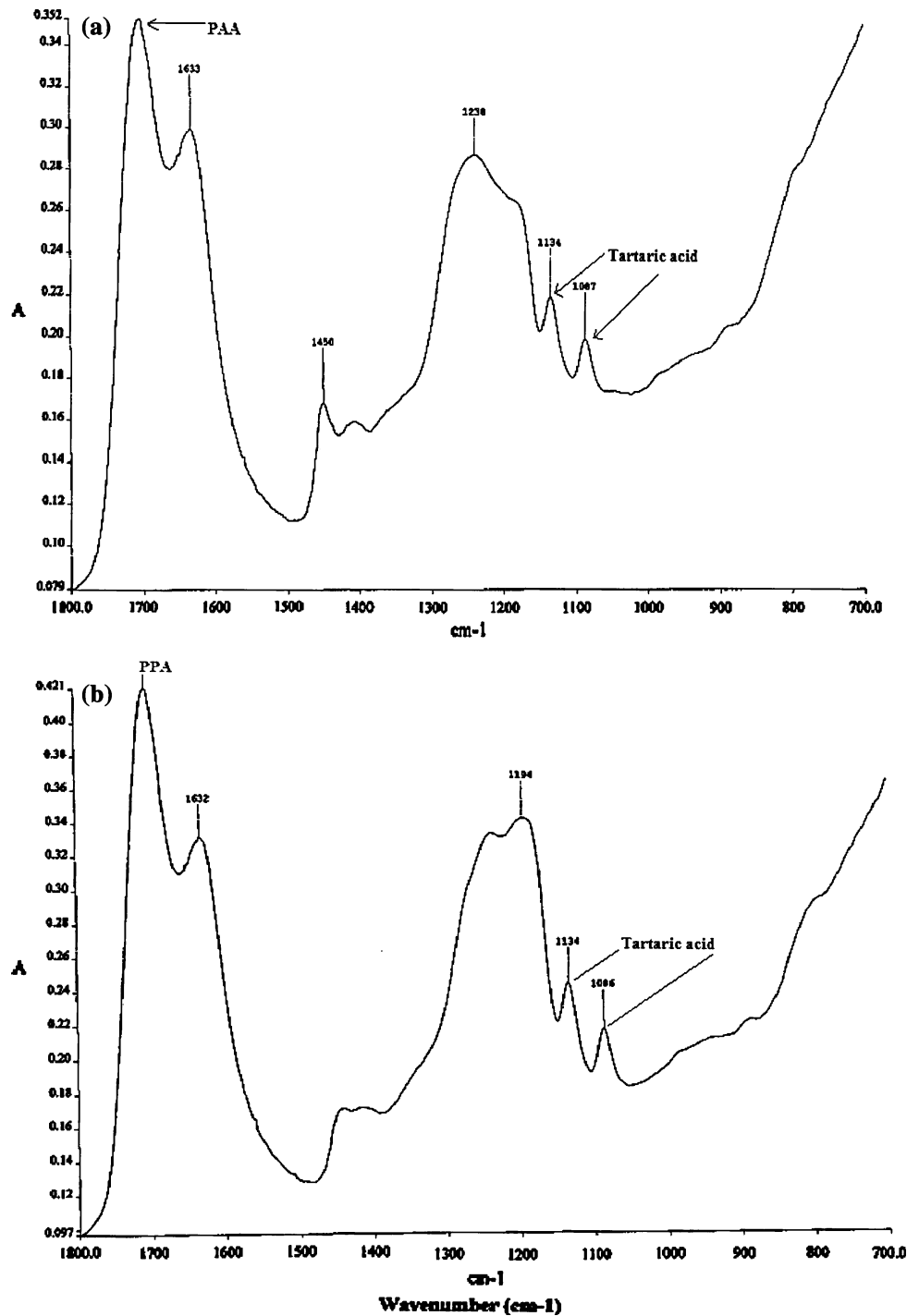
Spectra were generated at 2, 5, 10, 30 and at 60 min after the start of mixing for all the samples. For both cements the COOH peak was measured at  $1,700\text{ cm}^{-1}$  with  $\text{COO}^-$  peaks measured at  $1,600\text{ cm}^{-1}$  and  $1,410\text{ cm}^{-1}$  for Fuji IX and at  $1,560\text{ cm}^{-1}$  and  $1,405\text{ cm}^{-1}$  for Ketac Molar. Absorption spectra were obtained for the liquids of both Fuji IX Fast and Ketac Molar to compare with the spectra of setting cements and are shown in Fig. 2a and b.

## 3 Results

### 3.1 Spectra for non ultrasound (NUS) Ketac Molar and Fuji IX Fast

Spectra were obtained at 2, 5, 10, 30 and 60 min after mixing samples of Fuji IX Fast and Ketac Molar set without the application of ultrasound (NUS) are shown in shown in Fig. 3a and b. From the FTIR spectra the ratios of the heights of the  $1,600$  to  $1,700\text{ cm}^{-1}$  and the  $1,410$  to  $1,700\text{ cm}^{-1}$  peak were calculated for Fuji IX and heights of the  $1,560\text{ cm}^{-1}$  to  $1,700\text{ cm}^{-1}$  and the  $1,405$  to  $1,700\text{ cm}^{-1}$  peak were calculated for Ketac Molar. The setting reaction

**Fig. 2** Spectra for the liquid phase of (a) Fuji IX and (b) Ketac Molar



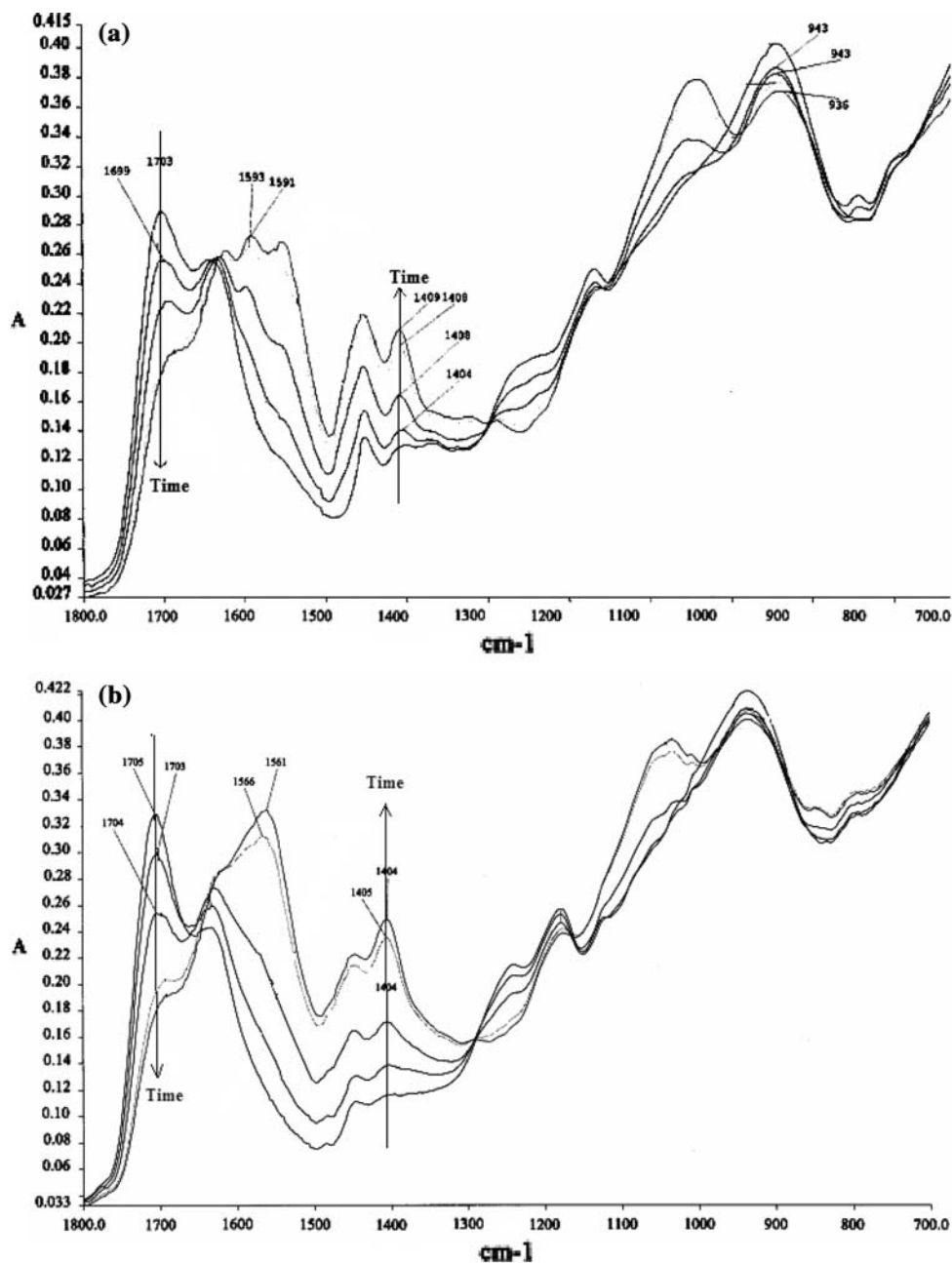
tends to a reduction in the number of COOH groups as they set and reform as COO<sup>-</sup> groups.

From the spectra the ratios of the peaks 1,600 cm<sup>-1</sup> and 1,410 cm<sup>-1</sup> to the 1,700 cm<sup>-1</sup> peak were calculated for Fuji IX and the ratios of 1,560 cm<sup>-1</sup> and 1,405 cm<sup>-1</sup> to 1,700 cm<sup>-1</sup> for Ketac Molar and are show in Fig. 4. At 2 and 5 min after mixing the peak ratios were higher for Fuji IX than Ketac molar, however at 30 and 60 min they were higher for Ketac Molar.

### 3.2 Effect of US application

Fuji IX showed increased setting on the application of US. The effect of US was dependent on the duration of US applied. Applying US for 15 s increased the rate of reaction; however at the end of 60 min after mixing the difference between the setting of non-ultrasound samples and samples with 15 s US application was not significant as shown in Table 1. Like Fuji IX, Ketac Molar also showed higher

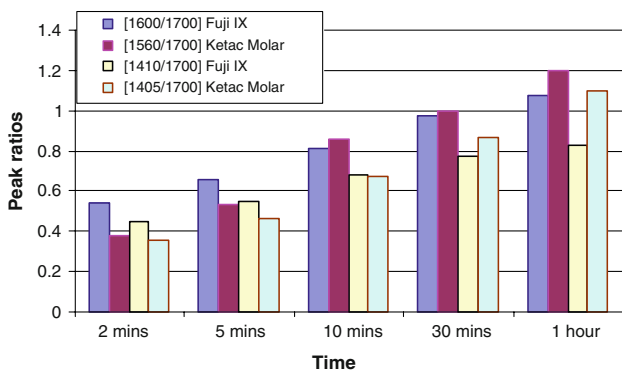
**Fig. 3** FTIR spectra for (a) Fuji IX and (b) Ketac Molar with no Ultrasound applied taken at 2, 5, 10, 30 and 60 min after mixing. The arrows indicate the increase or decrease in the heights of specific peaks with increasing time



setting rate on applying US and the setting was increased on increasing the duration of US as shown in Table 2.

The rate of setting increased with the increase in the duration of US application. Highest rate of setting was achieved on applying US for 55 s, the longest US application used in this study. When US was applied for 55 s, the peaks at  $1,700\text{ cm}^{-1}$  and  $1,405\text{ cm}^{-1}$  corresponding to COOH and  $\text{COO}^-$  respectively do not subsequently change much, indicating that polyacrylic acid (PAA) has already been neutralized by the ions from the glass phase and the cement is set.

Fuji IX samples showed higher  $\text{COO}^-/\text{COOH}$  ratios when the US application was started at 40 s after mixing rather than at 30 s after mixing. The ratios for Fuji IX with US starting at 30 and 40 s time after mixing are shown in Fig. 5a, the total duration of US application was 25 s. Ketac Molar samples also showed higher  $\text{COO}^-/\text{COOH}$  ratios when the US application was started at 40 s after mixing rather than at 30 s after mixing. The ratios for Ketac Molar with ultrasound starting at 30 and 40 s time after mixing are shown in Fig. 5b, the total duration of US application was 25 s.



**Fig. 4** COO<sup>-</sup>/COOH ratios of Fuji IX and Ketac Molar with no application of ultrasound

Applying US on both Ketac Molar and Fuji IX Fast increases their rate of setting, however the effect is greater in the case of Ketac Molar. On calculating the peak ratios

2 min after mixing and with various duration of US application it is obvious that Ketac Molar has enhanced set compared to Fuji IX Fast. However in the case of 15 s US application, the peak ratios at 2 min are higher for Fuji IX Fast, as shown in Fig. 6a.

When the ratios are obtained at 60 min after mixing, they clearly show increase setting for Ketac Molar than Fuji IX even with only 15 s of US. This also supports the fact that as the time increases the COO<sup>-</sup> groups increase implying salt formation becomes more enhanced in Ketac Molar, as shown in Fig. 6b.

3.3 Effect of section thickness

FTIR readings were taken on the opposite side of the sample to which US was applied. To determine the penetration of US two thicknesses of the samples were used. Results showed high COO<sup>-</sup>/COOH ratios thus increased

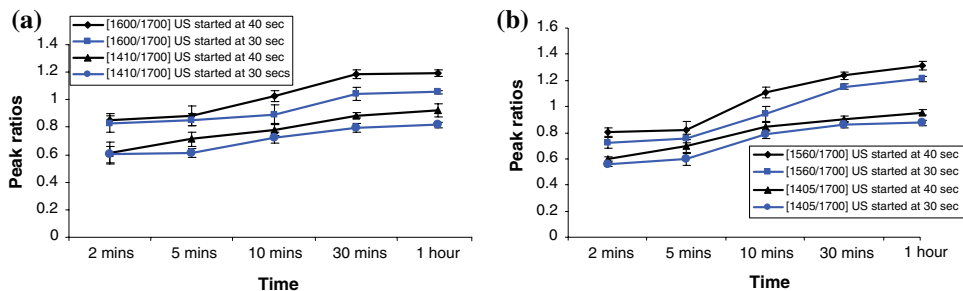
**Table 1** COO<sup>-</sup>/COOH ratios for Fuji IX at different times point after mixing with no ultrasound (NUS) and 15 (15 s US), 35 (35 s US) and 55 (55 s US) seconds of ultrasound application after 30 s after mixing

Time (min)	NUS		15 s US		35 s US		55 s US	
	(1,600/1,700)	(1,410/1,700)	(1,600/1,700)	(1,410/1,700)	(1,600/1,700)	(1,410/1,700)	(1,600/1,700)	(1,410/1,700)
2	0.544	0.444	0.864	0.602	1.102	0.853	1.388	1.102
5	0.661	0.549	0.886	0.625	1.164	0.866	1.404	1.113
10	0.809	0.676	0.977	0.713	1.187	0.913	1.416	1.133
30	0.977	0.777	1.070	0.790	1.218	0.967	1.409	1.128
60	1.073	0.830	1.09	0.831	1.236	0.997	1.419	1.136

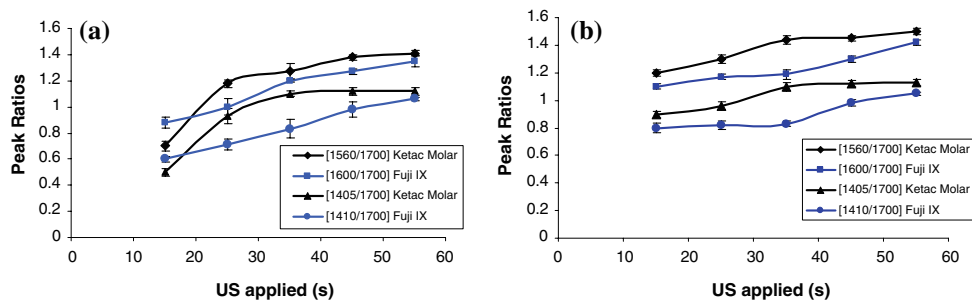
**Table 2** COO<sup>-</sup>/COOH ratios for Ketac Molar at different times point after mixing with no ultrasound (NUS) and 15 (15 s US), 35 (35 s US) and 55 (55 s US) seconds of ultrasound application after 30 s of mixing

Time (min)	NUS		15 s US		35 s US		55 s US	
	(1,560/1,700)	(1,405/1,700)	(1,560/1,700)	(1,405/1,700)	(1,560/1,700)	(1,405/1,700)	(1,560/1,700)	(1,405/1,700)
2	0.379	0.358	0.695	0.510	1.274	1.113	1.417	1.134
5	0.533	0.463	0.834	0.585	1.399	1.128	1.444	1.157
10	0.855	0.671	0.986	0.714	1.411	1.130	1.459	1.168
30	1.000	0.864	1.159	0.879	1.419	1.145	1.487	1.171
60	1.200	1.100	1.226	1.222	1.436	1.157	1.499	1.182

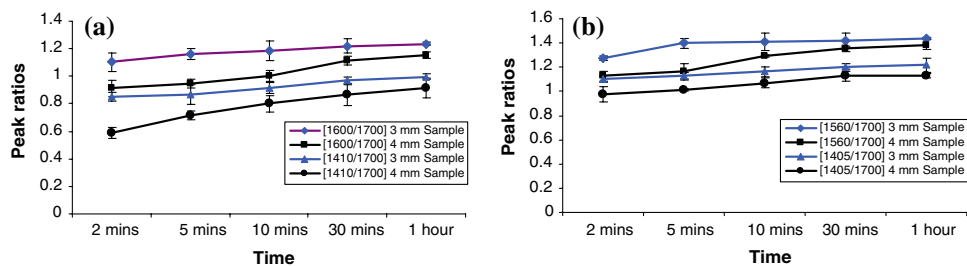
**Fig. 5** (a) Difference between COO<sup>-</sup>/COOH ratios of Fuji IX samples with ultrasound application started at 30 sec and 40 sec after mixing and applied for 25 s. (b) Difference between COO<sup>-</sup>/COOH ratios of Ketac Molar samples with ultrasound application started at 30 sec and 40 sec after mixing and applied for 25 s



**Fig. 6** (a) Peak ratios for Fuji IX Fast and Ketac Molar at 2 min after mixing with different durations of ultrasound applied. (b) Peak ratios for Fuji IX Fast and Ketac Molar at 60 min after mixing with different durations of ultrasound applied



**Fig. 7** (a) and (b) Difference between  $\text{COO}^-/\text{COOH}$  ratios of 3 and 4 mm thick Fuji IX and Ketac Molar samples with 35 s ultrasound application



setting for 3 mm samples ratios and neutralization of PAA at the end of 60 min after mixing as compared to 4 mm samples. As shown in the Fig. 7a the ratios for 3 mm samples are higher than for 4 mm samples on applying US for 35 s.

Higher ratios were achieved for Ketac Molar samples with 3 mm thickness as compared 4 mm thick samples as shown in Fig. 7b.

#### 4 Discussion

Increased rate and degree of setting was observed with increase of US duration from 15 to 55 s. The setting of the cements was higher when the US application was started at 40 s after mixing compared to starting 30 s after mixing, this finding has not been reported previously. This result shows that allowing the cement to set chemically for longer before application of US causes an increase production of  $\text{COO}^-$  groups in the cement which on application of US crosslink to give increase  $\text{COO}^-$  ratios.

Both Fuji IX and Ketac Molar showed higher rates of setting after applying US for at least 35 s. However the effect of US is more pronounced on Ketac Molar as compared to Fuji IX as shown in Fig. 6a. This figure shows the ratios at 2 min after mixing with different duration of US applied, it is obvious that the US has a greater effect on Ketac Molar at all US durations greater than 15 s. This supports the hypothesis that Fuji IX Fast sets faster during the initial minutes than Ketac Molar, as applying US for 15 s does not really affect and enhance the setting of this

cement. At the end of 60 min after mixing and with different durations of US application Ketac Molar shows higher values and thus increased setting as compared to Fuji IX as shown in Fig. 6b.

The effect of US was measured by placing the cement samples on the FTIR lens. The surface facing the FTIR lens was the surface opposite to the surface on which the US was applied. Thus to investigate the effect of thickness on penetration of US, US was applied to both 3 and 4 mm thick samples. Greater setting was observed for 3 mm samples as compared to 4 mm samples with all US application durations and with both starting time of 30 s and 40 s after mixing as shown in Fig. 7a and b. This tends to suggest that the effects of US are depth dependent, the greater the depth, the weaker effect of US at the bottom. However clinically the requirement is to set the occlusal surface quickly and to the greatest extent possible as the cement below the surface layer and within the tooth surface is less prone to moisture and desiccation.

Applying US not only increases the setting reaction of GICs, it also improves the mechanical properties of GIC [7]. The compressive strength and surface hardness of GIC has been shown to be increased by the application of US and creep can be minimized [8, 10]. Enhanced bond strength between GIC and enamel can be achieved by the application of US [11].

US application can be easily applied in dental clinics as it does not require any special instrument and can be applied by dentists using ultrasonic equipment used for scaling available in most of the dental clinics.

## 5 Conclusions

Ultrasound application accelerates the formation of the acid salts. The salt formation increased with increase time of US within the times investigated in this study. The effect of application of US to setting GICs is influenced by time of the start of application of the ultrasound. The effects appear to material specific, with Ketac Molar showing a greater effect than Fuji IX.

## References

1. R.T. Ramsden, R.C.D. Herdman, R.H. Lye, Ionomeric bone cement in neuro-otological surgery. *J. Laryngol. Otol.* **11**, 949–953 (1992)
2. I.M. Brook, P.V. Hatton, Glass-ionomers: bioactive implant materials. *Biomaterials* **6**, 565–571 (1998). doi:[10.1016/S0142-9612\(98\)00138-0](https://doi.org/10.1016/S0142-9612(98)00138-0)
3. A.M. Young, S.A. Rafeeka, J.A. Howlett, FTIR investigation of monomer polymerization and polyacid neutralization kinetics and mechanisms in various aesthetic dental restorative materials. *Biomaterials* **25**, 823–833 (2004). doi:[10.1016/S0142-9612\(03\)00599-4](https://doi.org/10.1016/S0142-9612(03)00599-4)
4. J.W. McLean, Glass ionomer cements. *Br. Dent. J.* **164**, 293–300 (1988). doi:[10.1038/sj.bdj.4806434](https://doi.org/10.1038/sj.bdj.4806434)
5. B.M. Culbertson, Glass-ionomer dental restoratives. *Prog. Polym. Sci.* **26**, 577–604 (2001). doi:[10.1016/S0079-6700\(01\)00006-5](https://doi.org/10.1016/S0079-6700(01)00006-5)
6. A.J. de Gee, R.N. van Duinen, A. Werner, C.L. Davidson, Early and long-term wear of conventional and resin-modified glass ionomers. *J. Dent. Res.* **75**, 1613–1619 (1996)
7. C.J. Kleverlaan, R.N.B. van Duinen, A.J. Feilzer, Mechanical properties of glass ionomer cements affected by curing methods. *Dent. Mater.* **20**, 45–50 (2004). doi:[10.1016/S0109-5641\(03\)00067-8](https://doi.org/10.1016/S0109-5641(03)00067-8)
8. M.R. Towler, A.J. Bushby, R.W. Billington, R.G. Hill, A preliminary comparison of the mechanical properties of chemically cured and ultrasonically cured glass ionomer cements, using nano-indentation techniques. *Biomaterials* **22**, 1401–1406 (2001). doi:[10.1016/S0142-9612\(00\)00297-0](https://doi.org/10.1016/S0142-9612(00)00297-0)
9. E. Twomey, M.R. Towler, C.M. Crowley, J. Doyle, S. Hampshire, Investigation into the ultrasonic setting of glass ionomer cements, Part II Setting times and compressive strengths. *J. Mater. Sci.* **39**, 4631–4632 (2004). doi:[10.1023/B:JMSE.0000034158.69184.84](https://doi.org/10.1023/B:JMSE.0000034158.69184.84)
10. D.A. Tanner, N. Rushe, M.R. Towler, Ultrasonically set glass polyalkenoate cements for orthodontic applications. *J. Mater. Sci. Mater. Med.* **17**, 313–318 (2006). doi:[10.1007/s10856-006-8229-7](https://doi.org/10.1007/s10856-006-8229-7)
11. T.J. Algera, C.J. Kleverlaan, A.J. de Gee, B. Prah-Andersen, A.J. Feilzer, The influence of accelerating the setting rate by ultrasound or heat on the bond strength of glass ionomers used as orthodontic bracket cements. *Eur. J. Orthod.* **27**, 472–476 (2005). doi:[10.1093/ejo/cji041](https://doi.org/10.1093/ejo/cji041)